

DEVELOPMENT OF A 2-SEGMENT FOOT MODEL FOR KINEMATIC MEASUREMENT OF MEDICAL GAIT ANALYSIS.

L. Bauer, M. Hamberger, W. Böcker, H. Polzer, SF. Baumbach

Department of Orthopaedics and Trauma Surgery, Musculoskeletal University Center Munich (MUM), University Hospital, LMU Munich

Introduction

Instrumented gait analysis using optical motion capturing (OMC) represents an essential tool in the prevention, diagnosis, and therapy of a wide range of medical conditions. The ankle and foot are represented by a three segments analysis (Oxford Foot Model (OFM)). However, gait analysis with OMC and OFM is time consuming and requires a large setup.

Inertial measurement units (IMU) could be a time efficient alternative with a good accuracy in the sagittal and moderate accuracy in the coronal and transverse planes [1, 2]. But the foot is only represented by one segment. This oversimplification of the foot does not allow a meaningful analysis for pathologies within the ankle and foot.

The aim of the study was therefore threefold:

- 1) Development of a 2-segment foot model
- 2) Assessing a norm data set
- 3) Evaluation of its reliability

Methods

The study was approved by the local ethics commission (#19-0177).

First, the existing model was amended by an additional IMU placed vertically onto the calcaneus (Fig. 1: 3). The position of the already existing IMUs (forefoot, shank, thigh, pelvis) remained unchanged (Fig. 1: 1, 2). This allowed the assessment of the three major joint axis (Figure 1: A, B, C).

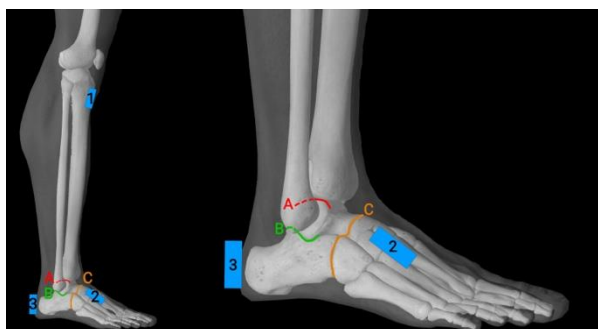


Figure 1: Illustration of the 2-segment foot model including the position of IMU on shank (1), forefoot (2) and hindfoot (3) as well as the three major joint axis: A) Ankle-, B) Subtalar-, C) Chopart-joint;

Second, a norm data set was established by measuring 20 healthy individuals without current or past injuries/pathologies within the foot or ankle.

Third, the intra-rater, inter-rater, and test-retest reliability was assessed on an additional 12 healthy subjects.

The assessment protocol for all subjects was identical. After the standardized application of the IMU sensors, a walking calibration was performed. Following a 2 min treadmill familiarization (4km/h), measurements were recorded for 30 seconds.

All subjects performed a total of 4 gait analysis: Day 1: One measurement by two independent observers; Day 2: Two measurements of each volunteer by one observer.

Data processing was performed in Matlab. Foot kinematics were calculated for tibia-forefoot, tibia-hindfoot, forefoot-hindfoot in sagittal, frontal, and transverse planes. All data were averaged over 100% gait cycle for all subjects. Intra-rater, Inter-rater and test-retest reliability was tested with statistic parametric mapping (SPM).

Results

The positioning of the additional sensor has proven to be stable. Figure 2 shows the mean kinematic values for the reference population. The SPM showed no significant differences for inter-rater, intra-rater, test-retest reliability ($p > 0.05$).

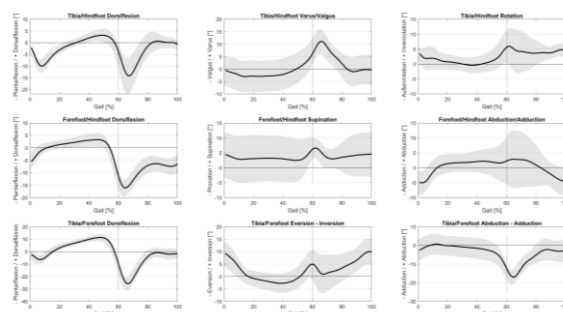


Figure 2: Kinematics of foot for sagittal, frontal, and transversal plane, mean (± 1 SD) values for 20 healthy subjects.

Discussion

The development of a 2-segment foot model seems a valuable extension to the current IMU setup. It allows to generate kinematic curves comparable to the OFM (with OMC) with a good intra-rater, inter-rater and test-retest reliability. A validation of the new model to the OMC is currently in progress. In the future, the IMU technology might prove a cost and time efficient method for a valid clinical gait analysis.

References

1. Park et al., Sensors (Basel), 2021. 21(11).
2. Rekant et al., SSRN. 2022.

