

VALIDATION OF A DIGITAL TWIN TO QUANTIFY THE LEVEL OF MOTOR CONTROL SUBOPTIMALITY IN PATIENTS

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Introduction

Neuro-musculoskeletal (NMSK) models, personalized and informed by experimental data, enable to predict internal biomechanical quantities which may have high informative value but that are difficult to measure *in vivo*. Motor control strategies that deviate from the so-called optimal control (e.g. a solution that minimizes the metabolic cost or energy expenditure) may further emerge, which may not be observed otherwise. Hence, we developed a Digital Twin in Healthcare (DTH), named JointForce, which we intend to position as a tool to quantify the level of suboptimality in a patient's motor control. In first instance, JointForce models will be used to predict joint contact forces (JCF) using various approaches, i.e., classical static optimization (hypothesizing optimal muscle control) and EMG-assisted approach [1]. Before the JointForce DTH can be employed to assist clinical decision making, it requires to undergo proper validation. In this work we present a first validation of JointForce models, and their predictions, against the recording of instrumented knee implants from a public dataset [2].

Methods

Experimental data from the last four editions of the Knee Grand Challenge (KGC) [2] were employed in this study. Image-based MSK models were generated using an in-house pipeline that exploits the STAPLE toolbox [3] and nmsBuilder [4]. Muscle points extracted from a generic template [5] were mapped onto the reconstructed bony geometries and minimally adjusted in accordance with medical images. Muscle properties were scaled and tuned to ensure physiological muscle behaviour [6], or personalized with information from available experimental data (e.g., maximal isometric forces scaled with the physiological cross-sectional areas outlined on the images). Biomechanical simulations of level walking were performed in OpenSim (standard workflow, from inverse kinematics to static optimization) and CEINMS (EMG-assisted approach, following model calibration). Predicted knee JCFs were compared to the corresponding *in vivo* measurements in terms of RMSE and R^2 . Statistical significance, between JCF profiles, was computed using Statistical Parametrical Mapping ($\alpha=0.05$).

Results

We hereby report the preliminary results on data from the 6th KGC (Figure 1). The static optimization approach produced estimates that more closely approximated the implant data (RMSE=0.42±0.1BW), compared to predictions resulting from the EMG-assisted approach

(RMSE=0.88±0.06BW). However, the opposite was observed in terms of JCF profile similarity ($R^2=0.89±0.05$ for static optimization, $R^2=0.91±0.03$ for EMG-assisted approach).

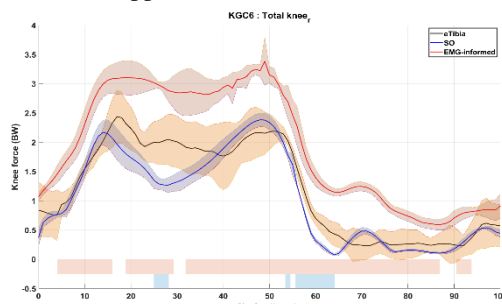


Figure 1: Knee joint contact forces predicted by the JointForce DTH, employing different approaches. Results are expressed in body weight (BW) and reported as mean and standard deviation across trials. *In vivo* recordings from an instrumented knee implant are reported for comparisons. Bars represent statistical significance ($p<0.05$).

Discussion

These first results are encouraging, although the overestimation associated to the use of the EMG-assisted approach requires further evaluation. The JointForce DTH is currently under validation using data from the other three editions of the KGC [2]. We expect to complete the validation in the next few weeks. Once the JointForce DTH is validated, we will identify a system (e.g., an index) to quantify the degree of neuromuscular suboptimality in a patient, based on the distance between the optimal solution (obtained via a static optimization) and the EMG-assisted solution.

References

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